



Detection of change in cancer breast tissues from fractal indicators:
A brief introduction

ANR MISTIC

Journées Textures à Vannes

October, 10 & 11 2024

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* Computational Modeling, Analysis of Imagery and Numerical Experiments

Overall mammographic density:

⇒ important risk factor for breast cancer radiological assessment

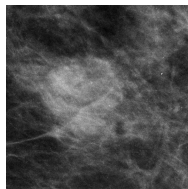
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Local fluctuations: self-similar textures ⇒ fractal analysis for

- classification of mammogram density (Caldwell et al., 1990, *Phys. Med. Biol.*)
- lesion detectability in mammograms (Burgess et al., 2001, *Med. Biol.*)
- assessment of breast cancer risk (Heine et al., 2002, *Acad. Radiol.*)

Mammogram



Tissue density fluctuations in normal vs. cancerous breasts

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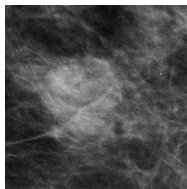
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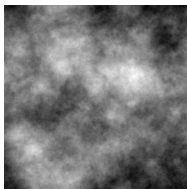
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Fractional Brownian fields: characterized by their local roughness

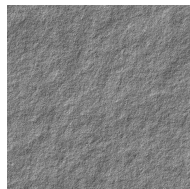
Mammogram



fractional Brownian field



stationary increments



Breast **microenvironment** plays a crucial role in tumorigenesis:

- structure integrity preserved \implies lesions are suppressed
- structure lost by tissue disruption \implies tumor is promoted

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Pioneer work: [Marin et al., 2017, *Med. Phys.*](#) quantitatively and objectively assessed

- tissue disruption
- loss of homeostasis in breast tissue microenvironment
- bilateral asymmetry

via wavelet-based mammogram local analysis.

Motivations and goals

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Main idea: quantify density fluctuations through the **Hurst exponent** estimated in

multifractal formalism based on 2D Wavelet Transform Modulus Maxima

\implies risk assessment and tumorous breasts detection without seeing a tumor

A very short reminder about fractional Brownian fields

fBf of Hurst exponent $H \in [0, 1]$ denoted $\{B_H(\mathbf{x}), \mathbf{x} \in \mathbb{R}^2\}$

- Gaussian field with zero-mean
- and for some $\sigma^2 > 0$, correlation function writing

$$\mathbb{E}[B_H(\mathbf{x})B_H(\mathbf{y})] = \frac{\sigma^2}{2} (\|\mathbf{x}\|^{2H} + \|\mathbf{y}\|^{2H} - \|\mathbf{x} - \mathbf{y}\|^{2H})$$

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- $H < 1/2$: anti-correlated
- $H = 1/2$: uncorrelated \implies disruption
- $H > 1/2$: long-range correlated

A very short reminder about fractional Brownian fields

Self-similarity

$$\forall \mathbf{h} \in \mathbb{R}^2, \lambda > 0, \quad B_H(\mathbf{x} + \lambda \mathbf{h}) - B_H(\mathbf{x}) \stackrel{(\text{law})}{\simeq} \lambda^H (B_H(\mathbf{x} + \mathbf{h}) - B_H(\mathbf{x}))$$

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Local regularity: same roughness everywhere $h(\mathbf{x}) \equiv H \implies$ monofractal signature

The larger the Hurst exponent H , the smoother the texture.

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Singularity spectrum: $\mathcal{D}(h)$ Hausdorff dimension of $\{\mathbf{x} \in \mathbb{R}^2, h(\mathbf{x}) = h\}$

$$\mathcal{D}(h) = \begin{cases} 2 & h = H \\ -\infty & h \neq H \end{cases}$$

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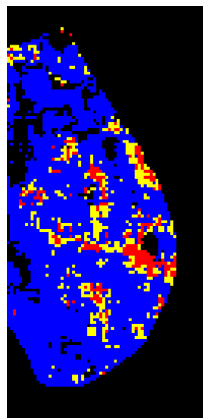
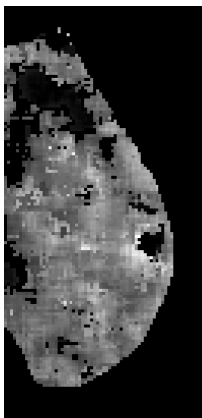
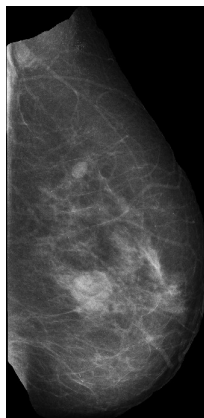
$$\mathcal{D}(h) = \begin{cases} 2 & h = H \\ -\infty & h \neq H \end{cases}$$

\implies estimation of $h, \mathcal{D}(h)$: multifractal formalism based on wavelet transform

Local fractal analysis of mammographic breast tissue

CompuMAINE local mammogram analysis (Marin et al., 2017, Phys. Med. Biol.)

- $H < 1/2$ monofractal anti-correlated: fatty tissues (healthy)
- $H > 1/2$ monofractal long-range correlated: dense tissues (healthy)
- $H \simeq 1/2$ monofractal uncorrelated: disrupted tissues (tumorous)



Assessment of the role of disruption in tumor promotion

Dataset: *University of South Florida*, Digital Database for Screening Mammography

- Mediolateral oblique views only;
- 43 normal, 49 cancer, 35 benign;
- for benign and cancer microcalcification only, masses excluded;

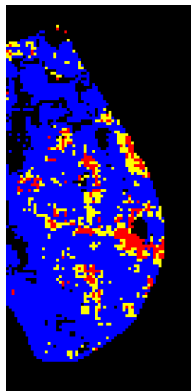


Image sliding-window analysis:

- squared 360×360 -pixel window
 - with 32-pixel horizontal and vertical shifts
- ⇒ analysis of all 360×360 -pixel overlapping patches

Example: mammogram of size 4459×2155 pixels

4457 patches \iff 4457 measures of the roughness H

Metric: number of yellow patches

$H \sim 1/2 \implies$ disrupted tissues

Q.: Is the quantity of disrupted tissues, $H \simeq 1/2$, indicative of a tumorous breast?

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Wilcoxon rank test a.k.a. Wilcoxon-Mann-Whitney

Independent sets of real numbers X and Y , of cardinalities n_x and n_y respectively

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If at least 20 samples, law of S_x well approximated by a Gaussian with

$$\mu = n_x n_y / 2; \quad \sigma^2 = n_x n_y (n_x + n_y + 1) / 2.$$

If $|S_x - \mu| / \sigma > 1.96$, **H0** is rejected with confidence level $\alpha = 0.05$.

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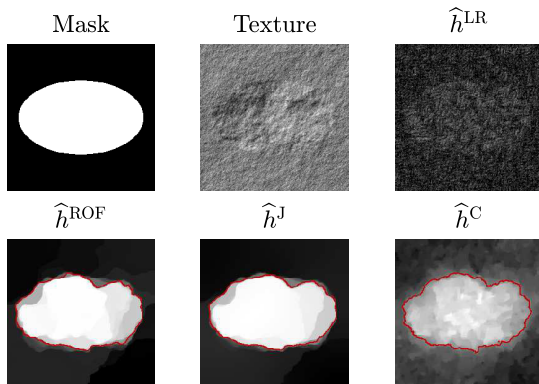
Tumorous breasts have **more disrupted tissues** compared to normal breasts:

normal vs. cancer: $P \sim 0.0423$, normal vs. benign: $P \sim 0.0009$.

Fractal features piecewise constant estimation from leaders

Pascal et al., 2020, *Ann. Telecommun.*; Pascal et al., 2021, *Appl. Comput. Harmon. Anal.*;
Pascal et al., 2021, *J. Math. Imaging Vis.* \implies *Journées ANR Mystic, April 2023*

$$\left(\widehat{\mathbf{h}}, \widehat{\mathbf{v}}\right) (\mathcal{L}; \lambda, \alpha) = \underset{\mathbf{h}, \mathbf{v}}{\operatorname{argmin}} \sum_a \|\log \mathcal{L}_{a,\cdot} - \log(a)\mathbf{h} - \mathbf{v}\|^2 + \lambda \mathcal{Q}(\mathbf{D}\mathbf{h}, \mathbf{D}\mathbf{v}; \alpha)$$



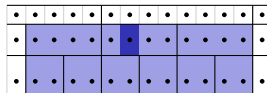
\implies estimation of the local regularity, i.e., roughness, at the **pixel** level

But first: assess that the wavelet leaders formalism agrees with WTMM on patches

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Wavelet leaders: $\mathcal{L}_{a,\underline{n}}$ at scale a and pixel \underline{n} supremum of wavelet coefficients

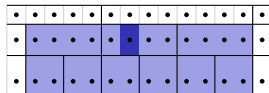
- at all finer scales $a' \leq a$
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For a grid of pixels $\Omega \subset \mathbb{R}^2$, scaling exponent $\tau(q)$ accessible through

$$\frac{1}{|\Omega|} \sum_{\underline{n} \in \Omega} \mathcal{L}_{a,\underline{n}}^q = F_q a^{\tau(q)}, \quad a \rightarrow 0^+$$

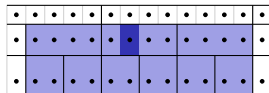
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linear regression to estimate H for all 360×360 -pixel overlapping patches

Wavelet leader coefficients (Wendt et al., 2009, Sig. Process.)

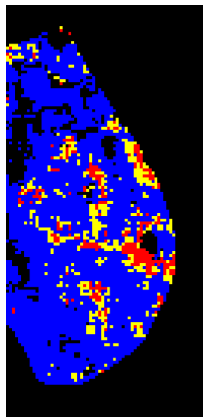
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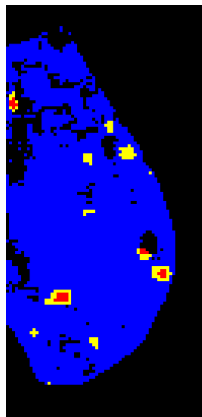
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CompuMaine



Leaders

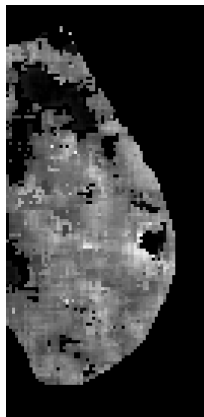


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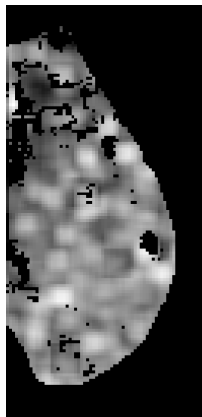
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Multifractal analysis of mamographic microenvironment

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2D Wavelet Transform: $\{f(\mathbf{x}), \mathbf{x} \in \mathbb{R}^2\}$ 2D-field

Smoothing function $\varphi(\mathbf{x}) \implies$ wavelets $\psi_1(\mathbf{x}) = \partial_{x_1}\varphi(x_1, x_2)$, $\psi_2(\mathbf{x}) = \partial_{x_2}\varphi(x_1, x_2)$

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Example: Gaussian and Mexican hat smoothing functions

$$\varphi_{\text{Gauss}}(\mathbf{x}) = \exp(-\|\mathbf{x}\|^2/2); \quad \varphi_{\text{Mex}}(\mathbf{x}) = (2 - \|\mathbf{x}\|^2) \exp(-\|\mathbf{x}\|^2/2)$$

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Wavelet Transform Modulus Maxima

$$\{(\mathbf{b}, a) \in \mathbb{R}^2, \times \mathbb{R}_+^*\} \quad \mathbf{M}_\psi[f](\mathbf{b}, a) \text{ locally maximal in direction } \mathbf{A}_\psi[f](\mathbf{b}, a)\}$$

Multifractal framework: Wavelet Transform Modulus Maxima

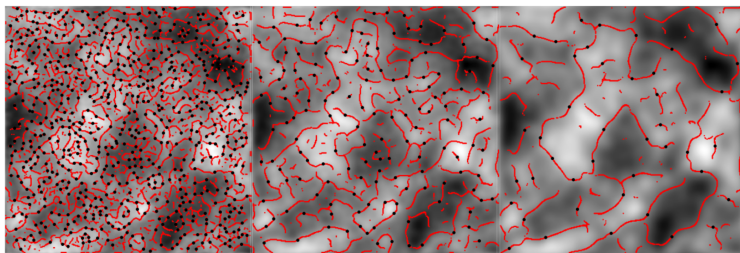


Figure 4.2: The maxima chains are shown for scales $a = 2^1\sigma_w$ (left), $a = 2^2\sigma_w$ (middle), and $a = 2^3\sigma_w$ (right) (where $\sigma_w = 7$ pixels) overlaid onto a 2D fBm image with $H = 0.5$. The local maxima along \mathcal{M}_ψ (WTMMM) are shown through small filled black dots.

Source: Basel G. White

Multifractal framework: Wavelet Transform Modulus Maxima

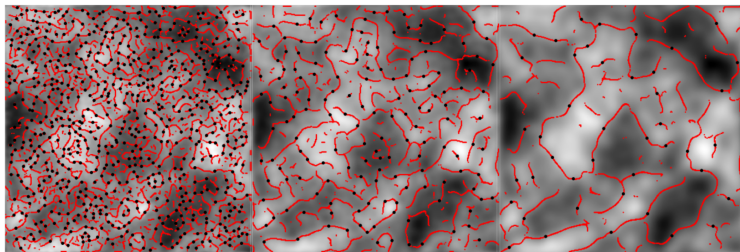


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Wavelet Transform space-scale skeleton: $\mathcal{L}(a)$

lines formed by WTMM maxima across scales

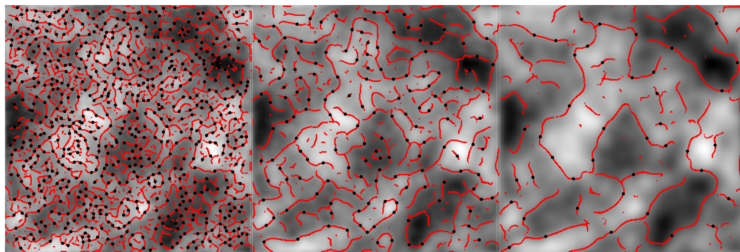


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lines formed by WTMM maxima across scales

If a maxima line $\mathcal{L}_{x_0}(a)$ is pointing toward a singularity x_0 as $a \rightarrow 0^+$, then

$$\mathbf{M}_\psi[f](\mathcal{L}_{x_0}(a)) \sim a^{h(x_0)}, \quad a \rightarrow 0^+$$

provided that the wavelet has $n_\psi > h(x_0)$ vanishing moments.

Partition function: for a set $\mathcal{L}(a)$ of maxima lines

$$\mathcal{Z}(q, a) = \sum_{\ell \in \mathcal{L}(a)} \left(\sup_{(\mathbf{b}, a') \in \ell, a' \leq a} \mathbf{M}_\psi[f](\mathbf{b}, a') \right)^q$$

q : statistical order moment

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q : statistical order moment

Roughness, quantified by Hölder exponent, characterized by $\tau(q)$ spectrum

$$Z(q, a) \sim a^{\tau(q)}, \quad a \rightarrow 0^+$$

For 2D fractional Brownian field: $\tau(q) = qH - 2$ is **linear**.

Partition function: for a set $\mathcal{L}(a)$ of maxima lines

$$Z(q, a) = \sum_{\ell \in \mathcal{L}(a)} \left(\sup_{(\mathbf{b}, a') \in \ell, a' \leq a} \mathbf{M}_\psi[f](\mathbf{b}, a') \right)^q$$

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Singularity spectrum: $\mathcal{D}(h)$ Hausdorff dimension of $\{\mathbf{x} \in \mathbb{R}^2, h(\mathbf{x}) = h\}$

$$\mathcal{D}(h) = \min_q (qh - \tau(q)) \quad (\text{Legendre transform of } \tau)$$

Numerically: unstable estimation of $\tau(q)$ and $\mathcal{D}(q)$

\implies Mean quantities in a **canonical** ensemble with Boltzmann weights

$$W_\psi[f](q, \ell, a) = \frac{\left| \sup_{(\mathbf{b}, a') \in \ell, a' \leq a} \mathbf{M}_\psi[f](\mathbf{b}, a') \right|^q}{\mathcal{Z}(q, a)}$$

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Roughness: robust local regularity estimation

$$h(q, a) = \sum_{\ell \in \mathcal{L}(a)} \ln (W_\psi[f](q, \ell, a)) W_\psi[f](q, \ell, a),$$

$$h(q) = \frac{d\tau}{dq} = \lim_{a \rightarrow 0^+} \frac{h(q, a)}{\ln a}$$

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Local fractal analysis of mammographic breast tissue

Roughness: $h(q) = \lim_{a \rightarrow 0^+} \frac{h(q, a)}{\ln a}$; **Singularity spectrum:** $\mathcal{D}(q, a) = \lim_{a \rightarrow 0^+} \frac{\mathcal{D}(q, a)}{\ln a}$

- The larger the patch, the larger the range of q values, the better the estimate;
 - but risk of confusing average of several monofractal signatures and multifractal.
- ⇒ estimation on overlapping patches of size 360×360 pixels with 32-pixel shift

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Image sliding window analysis

1. Check that the central 256×256 pixels are contained in the mask;
2. if so, compute the Wavelet Transform for 50 scales, from $a = 7$ to 120 pixels;
3. extract the space-scale skeleton from the central 256×256 pixels;
4. compute $h(q, a)$ and $\mathcal{D}(q, a)$ from the partition function $\mathcal{Z}(q, a)$;
5. linear regressions $h(q, a)$ vs. $\log_2(a)$ and $\mathcal{D}(q, a)$ vs. $\log_2(a)$:

how to choose the range of scales $[a_{\min}, a_{\max}]$?

Local fractal analysis of mammographic breast tissue

For **each** patch of 360×360 pixels, i.e., 15.5×15.5 mm

$$\text{roughness: } h(q) = \lim_{a \rightarrow 0^+} \frac{h(q, a)}{\ln a}; \quad \text{singularity spectrum: } \mathcal{D}(q, a) = \lim_{a \rightarrow 0^+} \frac{\mathcal{D}(q, a)}{\ln a}$$

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The Autofit Methodology: imposing $\log_2 a_{\max} - \log_2 a_{\min} \geq 1$ explore

$$\log_2 \frac{a_{\min}}{\sigma_w} = 0.0, 0.1, \dots, 2.1, \quad \log_2 \frac{a_{\max}}{\sigma_w} = 2.0, 2.1, \dots, 4.1, \quad \text{with } \sigma_w = 7 \text{ pixels}$$

and select $[a_{\min}, a_{\max}]$ if and only if

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and select $[a_{\min}, a_{\max}]$ if and only if

- linear regression on $h(q=0, a)$ from a_{\min} to a_{\max} yields

$$-0.2 < \hat{h}(q=0) = \hat{H} < 1$$

- $H \leq -0.2$: high roughness \implies abnormally high noise
- $H \geq 1$: low roughness, differentiable field \implies artificially smooth

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- linear regression on $\mathcal{D}(q=0, a)$ from a_{\min} to a_{\max} yields

$$1.7 < \widehat{\mathcal{D}}(h(q=0)) < 2.5$$

for a monofractal field of Hurst exponent H , expected to be $\mathcal{D}(H) = 2$

but finite size effect affect the maxima lines as $a \rightarrow 0^+$

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and select $[a_{\min}, a_{\max}]$ if and only if

- coefficient of determination of linear regression on $h(q = 0, a)$ from a_{\min} to a_{\max}

$$R^2 > 0.96$$

sufficiently linear to extract the Hurst exponent H

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and select $[a_{\min}, a_{\max}]$ if and only if

- weighted standard deviation across q of the $\hat{h}(q)$ estimated from a_{\min} to a_{\max}

$$\text{sd}_w < 0.06$$

\implies excludes multifractal scaling

q	-2	-1.5	-1	-0.5	-0.3	-0.2	-0.1	0	0.1	0.2	0.3	0.5	1	1.5	2	2.5	3
w	0.1	0.5	1	3	5	7	9	10	9	8	7	5	3	2	1	0.5	0.2

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and select $[a_{\min}, a_{\max}]$ if and only if

- weighted average of goodness of fit of $\hat{h}(q)$ estimated from a_{\min} to a_{\max}

$$\langle R_w^2 \rangle > 0.96$$

\implies ensures self-similarity

q	-2	-1.5	-1	-0.5	-0.3	-0.2	-0.1	0	0.1	0.2	0.3	0.5	1	1.5	2	2.5	3
w	0.1	0.5	1	3	5	7	9	10	9	8	7	5	3	2	1	0.5	0.2

Local fractal analysis of mammographic breast tissue

For **each** patch of 360×360 pixels:

\implies linear regressions $h(q, a)$ vs. $\log_2(a)$ and $\mathcal{D}(q, a)$ vs. $\log_2(a)$ across $[a_{\min}, a_{\max}]$

The Autofit Methodology: imposing $\log_2 a_{\max} - \log_2 a_{\min} \geq 1$ explore **418 couples**

$$\log_2 \frac{a_{\min}}{\sigma_w} = 0.0, 0.1, \dots, 2.1, \quad \log_2 \frac{a_{\max}}{\sigma_w} = 2.0, 2.1, \dots, 4.1, \quad \text{with } \sigma_w = 7 \text{ pixels}$$

and select $[a_{\min}, a_{\max}]$ if and only if

- $-0.2 < h(q=0) < 1$: expected roughness
- $1.7 < \hat{D} < 2.5$: expect 2
- $R^2 > 0.96$: accurate estimation of H
- $sd_w < 0.06$: monofractal scaling
- $\langle R_w^2 \rangle > 0.96$: $h(q, a)$ sufficiently linear

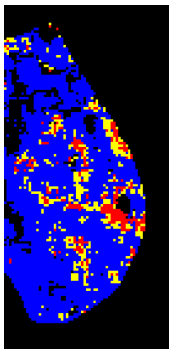
\implies If no scale range $[a_{\min}, a_{\max}]$ for which all conditions are satisfied: **no scaling**.

Local fractal analysis of mammographic breast tissue

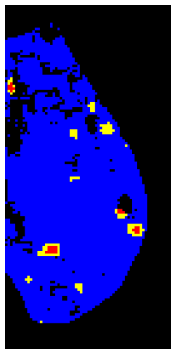
Wavelet leader coefficients (Wendt et al., 2009, Sig. Process.)

- $H < 1/2$ monofractal anti-correlated: fatty tissues (healthy)
- $H > 1/2$ monofractal long-range correlated: dense tissues (healthy)
- $H \simeq 1/2$ monofractal uncorrelated: disrupted tissues (tumorous)

CompuMaine



fixed scales



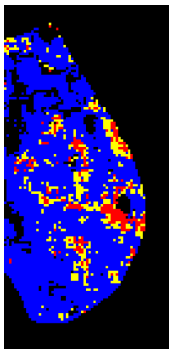
$$[a_{\min}, a_{\max}] = [2^3, 2^5]$$

Local fractal analysis of mammographic breast tissue

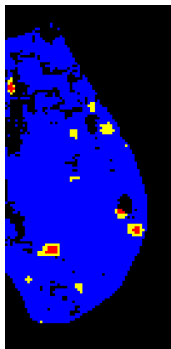
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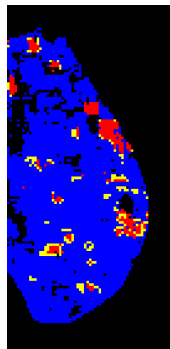
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fixed scales



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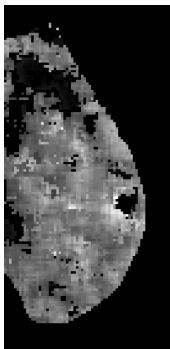
$$[a_{\min}, a_{\max}] = [2^3, 2^5] \quad [a_{\min}, a_{\max}] \subset [2^2, 2^8]$$

Local fractal analysis of mammographic breast tissue

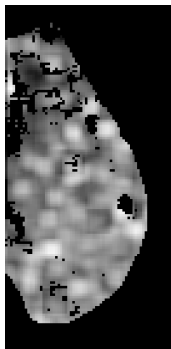
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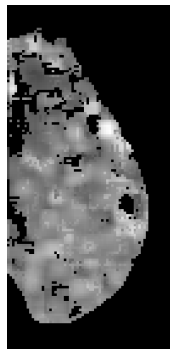
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Marin et al., 2017, *Phys. Med. Biol.*

DDSM: *University of South Florida*, Digital Database for Screening Mammography

43 normal vs. 49 cancer, 35 benign

⇒ digitized films: lossless LJPEG 12-bit images (pixel values: integers in [0, 4095])

Tumorous breasts have more disrupted tissues compared to normal breasts:

normal vs. cancer: $P \sim 0.0423$, normal vs. benign: $P \sim 0.0009$.

Mammogram datasets

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Russian: *Perm Regional Oncological Dispensary*

81 cancer vs. 23 benign

⇒ digitally acquired mammograms: uncompressed 8-bit BMP images ([0, 255])

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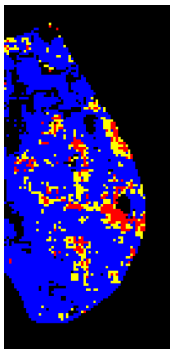
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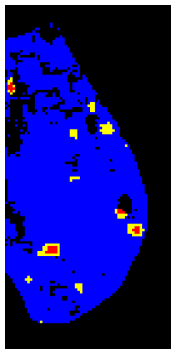
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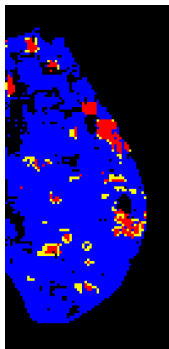
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Wavelet leaders with

- Daubechies wavelets with $n_\psi = 2$ vanishing moments
- \sim scales selected by the CompuMaine autofit method, up to rounding errors

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cancer vs. benign: $P \sim 0.074$

Patch-wise fractal analysis of mammograms with WT modulus maxima method

- disrupted tissues, characterized by $H \sim 1/2$, indicate loss of homeostasis
- quantity of disrupted tissues discriminates between

(Marin et al., 2017) tumorous vs. normal $P \sim 0.0006$

(Gerasimova-Chechkina et al., 2021) cancer vs. benign $P \sim 0.0030$

⇒ exploration of 418 couples of (a_{\min}, a_{\max}) for each patch and strict conditions

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⇒ exploration of 418 couples of (a_{\min}, a_{\max}) for each patch and **strict** conditions

Reproduction with wavelet leaders formalism on Russian dataset

- range of scales for each patch extracted from CompuMaine analyses,
- remains less informative: $P \sim 0.0740$

From patch-wise to pixel-wise fractal analysis

- using wavelet leaders framework,
- combined with variational methods,
- with PyTorch implementation to benefit from fast GPU computing,
- reduced number of hyperparameters & fine-tuned automatically

⇒ increase the sensibility in the measurement of the quantity of disrupted tissues

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Asymmetry in tissue disruption in cancerous cases

- assessed both in Marin et al., 2017 and Gerasimova-Chechkina et al., 2021,
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Anisotropic Gaussian fields for mammogram modeling

- observed in Richard & Biermé, 2010
- many tools that have never been applied to mammogram yet!